

## Central Lancashire Online Knowledge (CLoK)

Title	Particle release from implantoplasty of dental implants and impact on cells
Type	Article
URL	<a href="https://clock.uclan.ac.uk/34765/">https://clock.uclan.ac.uk/34765/</a>
DOI	<a href="https://doi.org/10.1186/s40729-020-00247-1">https://doi.org/10.1186/s40729-020-00247-1</a>
Date	2020
Citation	Barrak, Fadi N, Li, Siwei, Muntane, Albert and Jones, Julian R. (2020) Particle release from implantoplasty of dental implants and impact on cells. International Journal of Implant Dentistry, 6 (50).
Creators	Barrak, Fadi N, Li, Siwei, Muntane, Albert and Jones, Julian R.

It is advisable to refer to the publisher's version if you intend to cite from the work.  
<https://doi.org/10.1186/s40729-020-00247-1>

For information about Research at UCLan please go to <http://www.uclan.ac.uk/research/>

All outputs in CLoK are protected by Intellectual Property Rights law, including Copyright law. Copyright, IPR and Moral Rights for the works on this site are retained by the individual authors and/or other copyright owners. Terms and conditions for use of this material are defined in the <http://clock.uclan.ac.uk/policies/>

RESEARCH

Open Access



# Particle release from implantoplasty of dental implants and impact on cells

Fadi N. Barrak<sup>1†</sup>, Siwei Li<sup>1†</sup>, Albert M. Muntane<sup>2</sup> and Julian R. Jones<sup>1\*</sup> 

## Abstract

**Background:** With increasing numbers of dental implants placed annually, complications such as peri-implantitis and the subsequent periprosthetic osteolysis are becoming a major concern. Implantoplasty, a commonly used treatment of peri-implantitis, aims to remove plaque from exposed implants and reduce future microbial adhesion and colonisation by mechanically modifying the implant surface topography, delaying re-infection/colonisation of the site. This in vitro study aims to investigate the release of particles from dental implants and their effects on human gingival fibroblasts (HGFs), following an in vitro mock implantoplasty procedure with a diamond burr.

**Materials and methods:** Commercially available implants made from grade 4 (commercially pure, CP) titanium (G4) and grade 5 Ti-6Al-4V titanium (G5) alloy implants were investigated. Implant particle compositions were quantified by inductively coupled plasma optical emission spectrometer (ICP-OES) following acid digestion. HGFs were cultured in presence of implant particles, and viability was determined using a metabolic activity assay.

**Results:** Microparticles and nanoparticles were released from both G4 and G5 implants following the mock implantoplasty procedure. A small amount of vanadium ions were released from G5 particles following immersion in both simulated body fluid and cell culture medium, resulting in significantly reduced viability of HGFs after 10 days of culture.

**Conclusion:** There is a need for careful evaluation of the materials used in dental implants and the potential risks of the individual constituents of any alloy. The potential cytotoxicity of G5 titanium alloy particles should be considered when choosing a device for dental implants. Additionally, regardless of implant material, the implantoplasty procedure can release nanometre-sized particles, the full systemic effect of which is not fully understood. As such, authors do not recommend implantoplasty for the treatment of peri-implantitis.

**Keywords:** Gingival, Fibroblast, Dental implants, Peri-implantitis, Implantoplasty, Titanium, Titanium alloy, Vanadium, Toxicity

## Background

Dental implants offer a viable long-term treatment option for patients with missing teeth [1, 2]. The use of metallic dental implants has relatively high reliability and long-term success rates; however, it is not without complications and the need for ongoing maintenance persists. Particles are generated during the life span of

an implant, and this can have significant physiological implications such as disrupted osseointegration and bone resorption (osteolysis) that may in turn lead to implant loss [3, 4]. Particles can be released during implant bed preparation, from implant surface due to shear forces during fixture insertion, from implant-abutment interface due to wear and during functional loading [5, 6]. Exposure to the oral environment such as saliva, bacteria and chemicals such as fluoride can further facilitate the corrosion and degradation of titanium [7–9]. A wide range of 10 to 20 µm in sizes of the released particles were reported in several locations such as at implant

\* Correspondence: [julian.r.jones@imperial.ac.uk](mailto:julian.r.jones@imperial.ac.uk)

<sup>†</sup>F. Barrak and S. Li contributed equally to this work.

<sup>1</sup>Department of Materials, Imperial College London, South Kensington Campus, London SW7 2AZ, UK

Full list of author information is available at the end of the article

surface and peri-implant bone as well as distant sites such as the lungs, liver and kidney [5].

One common issue that can have detrimental impact on the long-term outcome of implant restorations and cause implant failure is peri-implantitis [10]. Peri-implantitis is a plaque-associated pathological condition occurring in tissues around dental implants [11]. It is characterised by inflammation in the peri-implant mucosa and subsequent progressive loss of surrounding supporting bone in which the implant is anchored. The risk of peri-implantitis is dependent on several of factors, and the frequency of peri-implantitis diagnosis has been reported to be 1–47% with selected implant systems [12, 13]. The large variation is due to the criteria used in diagnosis of peri-implantitis, e.g. some diagnose peri-implantitis with 0.5 mm crestal bone loss while at the other extreme 4 mm bone loss is needed for the diagnosis. Moderate to severe peri-implantitis (signs include bleeding on probing/suppuration and bone loss greater than 2 mm) was reported in 14.5% of patients [14]. Recently, the 2017 World Workshop Consensus report stated that in the absence of previous examination that records a diagnosis of peri-implantitis can be made with probing depths of greater than 6 mm and crestal bone loss greater than 3 mm in the presence of bleeding and/or suppuration on gentle probing. However, if previous records are available, then the diagnosis can be made with any increase in pocket depth with post remodelling bone loss of greater than 0.5 mm in the presence of bleeding and/or suppuration on gentle probing [11]. A number of studies suggested this inflammatory disease is associated with anaerobic plaque bacteria [15, 16]. It has also been suggested peri-implantitis can also be related to inadequate distribution of the chewing pressure on the tissues surrounding the implant, leading to the loosening of the artificial supports [17]. While plaque is the main risk factor, patients who have history of periodontal disease prior to implant treatment, and those with other risk factors such as poor oral hygiene, smoking or uncontrolled diabetes, also experienced higher rates of peri-implant disease [18, 19]. Additionally, there are also suggestions that peri-implantitis is the result of foreign body reaction [20].

Common treatment options for peri-implantitis include mechanical debridement (with or without antiseptic application) administration of local and systemic antibiotics or surgical techniques. It is well accepted that altering the affected implant surface is necessary to minimise the establishment of biofilm. Implantoplasty involves mechanically modifying the implanted threads (and the rough surface) that have become exposed in the patient's mouth, due to bone resorption, by removing the outer surface of the metal with rotary instruments,

in situ. The purpose is to reduce the roughness of the surface, and it is a commonly used technique to reduce plaque retention and prevent re-infection of the site [21, 22].

To the best of our knowledge, the release of particles from implants following implantoplasty procedure and their effect on cells has not been investigated. The purpose of this in vitro study was to assess the size, composition, ionic product release and biological impact of particles released from commonly used commercially pure grade 4 titanium and grade 5 titanium alloy implants following an implantoplasty procedure with diamond burr. This aims to raise the awareness of potential detrimental side effects of implantoplasty and the need for careful consideration of dental implant material.

## Materials and methods

### Materials

Reagents and solvents were purchased from Sigma-Aldrich (Dorset UK). Commercially pure grade 4 titanium implants ( $n = 3$ ) were purchased from Straumann (Sussex UK, Model number 021.4512, bone-level implant diameter 4.1 mm, Regular CrossFit®, SLA® 12 mm Roxolid®) (Fig. 1a). Grade 5 Ti-6Al-4 V titanium alloy implants were purchased from Biohorizons (Berkshire UK,  $n = 3$ , model number PBR50105, RBT 5.0 × 10.5 mm, 5.7 Platform) (Fig. 1d).

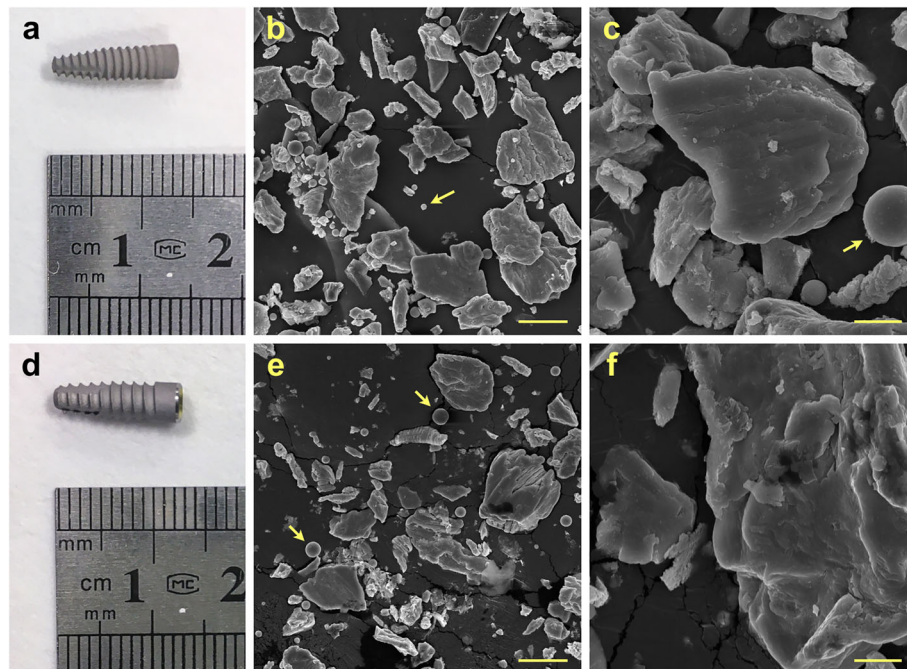
The methods in this study follow SPQR (standards for reporting qualitative research) guidelines.

### Mock implantoplasty protocol

Implants were secured with forceps held using table clamps. In order to minimise variations in the pressure applied during the implantoplasty, all procedures were completed by one operator. A handpiece (W&H, Alegria dental turbine handpieces TE-98 Led G) was used with motor set at 50,000 rpm. Diamond burrs (Diatech G856.314.021.9ML-200453AA) were limited to single use for 5 min on each implant. Particles released from implants following implantoplasty were collected, weighed and analysed for size, composition and ion release characteristics.

### Dynamic light scattering

Dynamic light scattering (DLS) was performed using a Malvern Zetasizer (instrument 2000) instrument to determine the size distribution of released implant particles. The instrument is equipped with a HeNe laser ( $\lambda = 632.8$  nm) with a backscattering detection angle of 173°. Particle size was also measured using Malvern Mastersizer (Malvern Panalytical Ltd, Royston, UK). Measurement duration (15 min) and number of sub-runs (3) were automatically adjusted by the instrument. Particles were suspended in 70% ethanol at a concentration of 5 mg ml<sup>-1</sup> and sonicated for 15 min prior to each measurement.



**Fig. 1** Representative photo of implants and SEM images of particles produced by mock implantoplasty procedure. **a–c** Straumann 021.4512, bone level, diameter 4.1 mm, regular CrossFit®, SLA® 12 mm Roxolid® (commercially pure grade 4 titanium). **d–f** Biohorizons PBR 50105, RBT 5.0 × 10.5 mm, 5.7 Platform (grade 5 titanium alloy). Arrows indicate titanium oxide spheres. Scale bar represents 20 and 5  $\mu\text{m}$  for low and high magnification respectively

### Scanning electron microscopy

Particle samples were dried in a 60 °C oven and secured to an aluminium sample holder with carbon tape and coated with 10 nm gold. Images were acquired using Zeiss Sigma-300 scanning electron microscope (SEM). For energy dispersive x-ray spectroscopy (EDX) analysis, samples were secured with silver conductive paint.

### Ion release from titanium particles

Simulated body fluid (SBF) was chosen as the dissolution test solution as we were interested in what happens when the particles become embedded in the soft/hard tissue rather than their interaction with saliva. SBF was prepared using the Kokubo method [23, 24]. Seven hundred millilitres of deionised (DI) water in a 1-L polypropylene beaker was warmed to 37 °C in a water bath. The reagents were slowly added to the DI water in the order given in [25], while the solution was continuously stirred. The pH was continuously monitored to avoid precipitation due to sudden increase. Once the reagents were mixed, the SBF was filled to 1 L with DI water. SBF was stored at 37 °C and used within 2 days. The pH was adjusted to 7.4 before use at 37 °C.

Grade 4 and 5 titanium (Ti) particles were suspended in SBF at concentrations of 0.75, 1.5 and 3  $\text{mg ml}^{-1}$  in airtight polyethylene containers, which were placed on an orbital shaker rotating at 120 rpm inside a 37 °C

incubator. One millilitre of aliquots was taken at day 0, 3 and 10 for the analysis of pH and ionic concentration.

### Cell culture and viability assay

Human gingival fibroblasts (HGFs) (PCS-201-018™, ATCC®, UK) were culture expanded in basal Dulbecco's modified Eagle's medium (DMEM) supplemented with 100 unit  $\text{ml}^{-1}$  penicillin, 100  $\mu\text{g ml}^{-1}$  streptomycin and 10% (v/v) foetal bovine serum (FBS) in standard tissue-culture flasks in a humidified atmosphere containing 5%  $\text{CO}_2$ . Upon confluence, cells were subcultured using 1× trypsin-EDTA (500  $\mu\text{g ml}^{-1}$  trypsin with 200  $\mu\text{g ml}^{-1}$  EDTA in Hank's Balanced Salt Solution).

To evaluate the potential cytotoxic effect of grade 4 and 5 Ti particles on HGFs, two groups of test samples were prepared for cell culture, the particles in media and the dissolution products of the particles. Ti particles were sterilised with 70% ethanol for 1 min before use. Group 1 (dissolution): grade 4 and 5 Ti particles were suspended in DMEM at concentrations of 0.75, 1.5 and 3  $\text{mg ml}^{-1}$  in airtight polyethylene containers, which were placed on an orbital shaker rotating at 120 rpm. inside a 37 °C incubator for 72 h. The media were filtered through 0.2  $\mu\text{m}$  PTFE membrane syringe filters following incubation to remove the particles before use in cell culture. Group 2 (particle): Sterilised grade 4 and 5 Ti particles were suspended in DMEM at concentrations of



0.75, 1.5 and 3 mg ml<sup>-1</sup> and used for cell culture without filtering. Basal DMEM and DMEM containing unprocessed grade 4 and 5 implants were used as controls. One millilitre of aliquots was taken at day 0, 3 and 10 for the analysis of pH and ionic concentration.

A 3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide (MTT) metabolic activity assay was performed to assess cellular metabolic activity of HGFs in response to group 1 and 2 test samples. Briefly, HGFs were seeded at 3000 cells cm<sup>-2</sup> in 24-well plates and allowed to grow for 24 h in basal DMEM. Basal medium was then replaced with the test samples supplemented with 10% FBS and cultured for a further 3, 7 or 10 days. At each time point, culture medium was replaced with 1 mg ml<sup>-1</sup> MTT in plain DMEM. MTT solution was removed after 3 h, and dimethyl sulfoxide (DMSO) was added to dissolve the formazan crystals formed by living cells. The luminescence of the resulting solutions was measured at 570 nm in a plate reader.

#### Inductively coupled plasma optical emission spectrometer (ICP-OES)

The elemental concentration of titanium, aluminium, iron and vanadium in the following media was determined using ICP-OES (iCaP6300 Duo, Thermo Fisher Scientific, UK) (1) SBF; (2) dissolution products of the particles from immersion in DMEM for 3 days (dissolution), and (3) DMEM sampled during the cell culture studies where cells were cultured with the particles (particle). Mixed standards of titanium, aluminium, iron and vanadium ions were prepared at 0, 2, 5, 20 and 40 ppm for calibration. All samples were run in triplicates, and an acid blank was incubated under the same conditions and used as a control.

#### Statistical analysis

Results were presented as mean  $\pm$  standard deviation (S.D.). Mann–Whitney *U* test (2 groups) or Mann–Whitney *U* test with Bonferroni correction (> 2 groups) was performed using OriginPro 2019. Results were deemed significant if the probability of occurrence by random chance alone was less than 5% (i.e.  $p < 0.05$ ).

#### Results

Particles released from implants following the mock implantoplasty procedure were collected, and microparticle size of particles produced from the grade 4 (G4) and grade 5 (G5) implants was  $77.4 \pm 9.1 \mu\text{m}$  (modal number 66.3  $\mu\text{m}$ ) and  $48.4 \pm 6.4 \mu\text{m}$  respectively (modal number 43.1  $\mu\text{m}$ ). DLS analysis showed nano-sized particles were also present: hydrodynamic diameters were  $125.4 \pm 10.9 \text{ nm}$  (modal number 109.3 nm) and  $57.74 \pm 2.66 \text{ nm}$  (modal number 52.1 nm) respectively. SEM images (Fig. 1) revealed that particles fragmented from

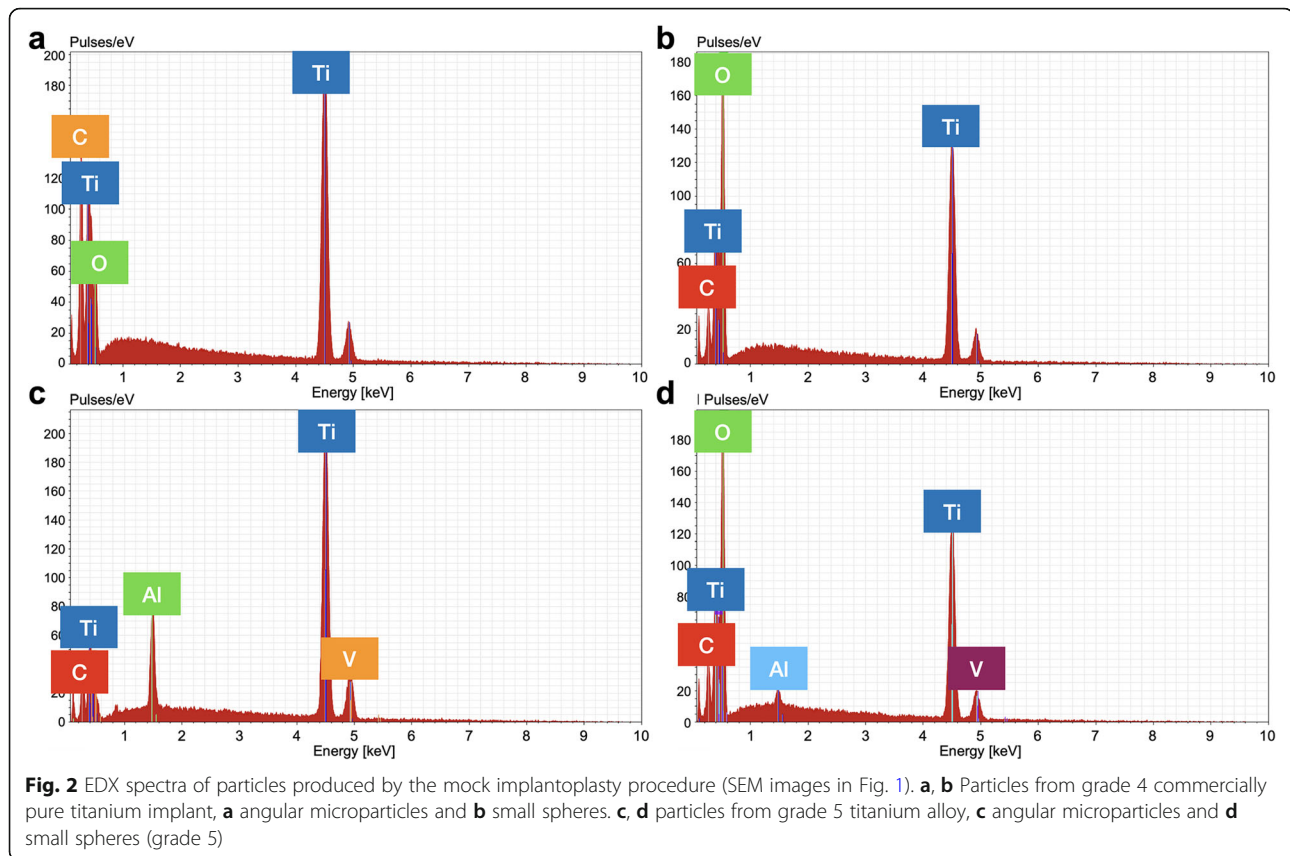
both G4 and G5 implants as the result of implantoplasty were irregular in shape and varied significantly in sizes. The elemental composition of the particles was analysed using EDX (Fig. 2). The EDX spectra demonstrated distinctive differences between G4 and G5 particles. In addition to titanium (Ti), both aluminium (Al) and vanadium (V) were detected in G5 particles. Carbon (C) was detected in both samples. According to EDX analysis, the spherical objects amongst implant particles (indicated by arrows in Fig. 1) were titanium oxide.

Release of ions from the G4 and G5 particles was first investigated in SBF (Fig. 3). Upon immersion, the release of Ti was minimal from both G4 and G5 particles in SBF. Release of V from G5 particles was detected by ICP only after 10 days of immersion. There was no noticeable release of aluminium (Al) and iron (Fe) ions. The pH of SBF remained at 7.4 during the immersion period. Similar results were observed when the particles were immersed in DMEM (Fig. 4), with low release of Ti and no noticeable release of aluminium Al and Fe from both G4 and G5 particles. V, up to  $0.116 \pm 0.023 \text{ ppm}$ , was only detected in medium containing G5 implant particles. Changing the concentration of the particles had little effect. As Al results were negligible, we assumed that no alloy particles passed through the 200-nm filters, but TiO<sub>2</sub> nanoparticles may have contributed to the Ti values (DLS measurement of blank media control returned value of 0).

The effect of G4 and G5 particles and their dissolution products on human gingival fibroblast viability in vitro was investigated using an MTT metabolic activity assay (Fig. 5). Administration of the dissolution products had no effect on cellular metabolic activity up to day seven, but there appeared to be a reduction in metabolic activity in cells exposed to G5 dissolution products by day 10, though it was not statistically significant. When the cells were exposed to G5 particles, metabolic activity significantly reduced as early as day 3. However, when cells were cultured with the G4 particles, there were no adverse effects. The significantly reduced metabolic activity as a result of exposure to G5 particles was observed at all-time points. Changing the concentration of the particles had little effect.

#### Discussion

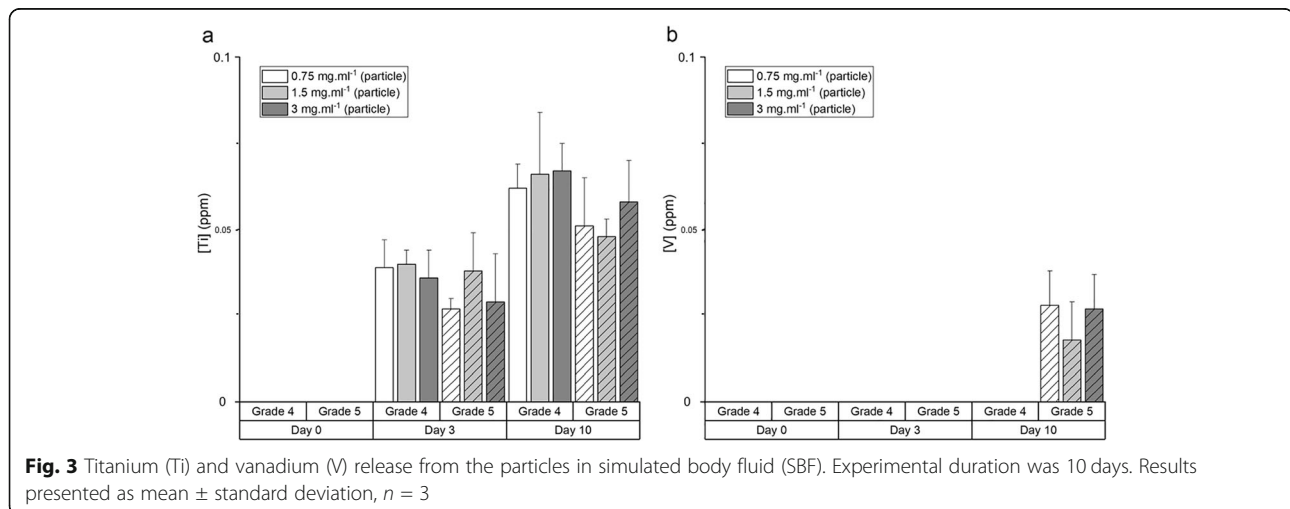
Unalloyed titanium, often referred to as commercially pure grade 4 titanium (CpTi), usually contains some trace elements of carbon, oxygen, nitrogen and iron (American Society for Testing and Materials international standards). These trace elements improve the mechanical properties of CpTi and are found in higher amounts from grade 1 to 4 CpTi [26]. Many dental implants are made from grade 4 (G4) CpTi, in order to improve its fatigue strength, and companies have also used

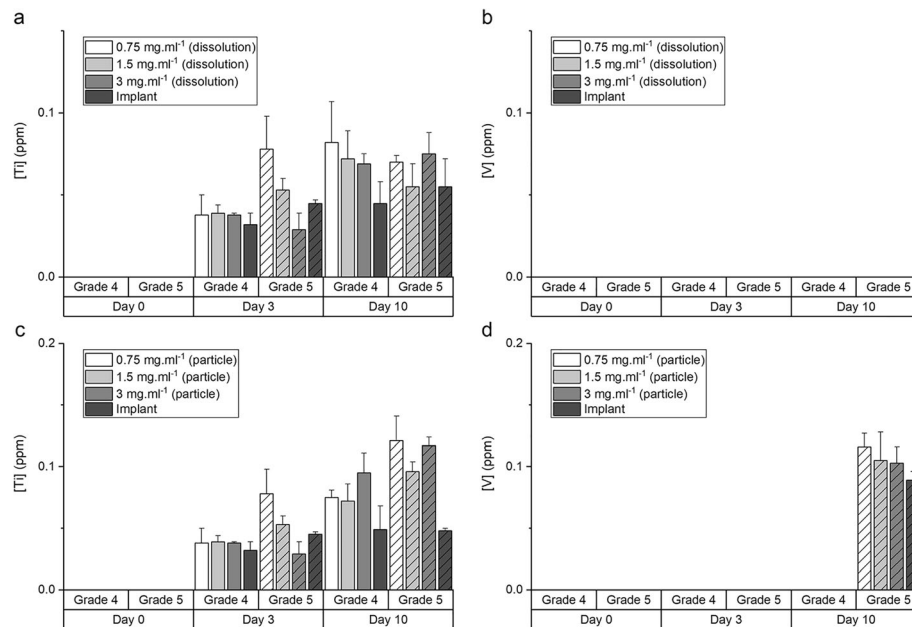


grade 5 (G5) titanium alloys (Ti-6Al-4 V), which contains metals including vanadium and aluminum.

In the present study, standardised implantoplasty procedure was performed on both G4 (Straumann, model number 021.4512, bone-level implant diameter 4.1 mm, Regular CrossFit®, SLA® 12 mm Roxolid®) and G5 (Bio-horizons, model number PBR50105, RBT 5.0 × 12 mm, 5.7 Platform) implants. Implant particles were released from both types of implants (Fig. 1). The smaller particle

size generated from G5 implants is likely to be due to the G5 alloy having a higher hardness. Typical G5 alloy has a hardness of 36 (HRC, Rockwell C) compared to 23 (HRC, Rockwell C) of G4 [27, 28]. Some TiO<sub>2</sub> spheres were detected. This is because when titanium implant surface is exposed to air, titanium oxide (TiO<sub>2</sub>) film is formed on the implant surface. This layer (1.5–10 nm thickness) is formed due to the high affinity of Ti for oxygen [29]. This in turn could contribute to a certain





**Fig. 4** Titanium (Ti) and vanadium (V) content in Dulbecco's Modified Eagle Medium (DMEM). **a, b** Dissolution products (media filtered through 0.2  $\mu$ m PTFE membrane following initial soaking of the particles for 3 days) and **c, d** DMEM sampled during cell culture studies where cells were cultured with the particles over a period of 10 days (particles removed prior to ICP measurement). Results presented as mean  $\pm$  standard deviation,  $n = 3$

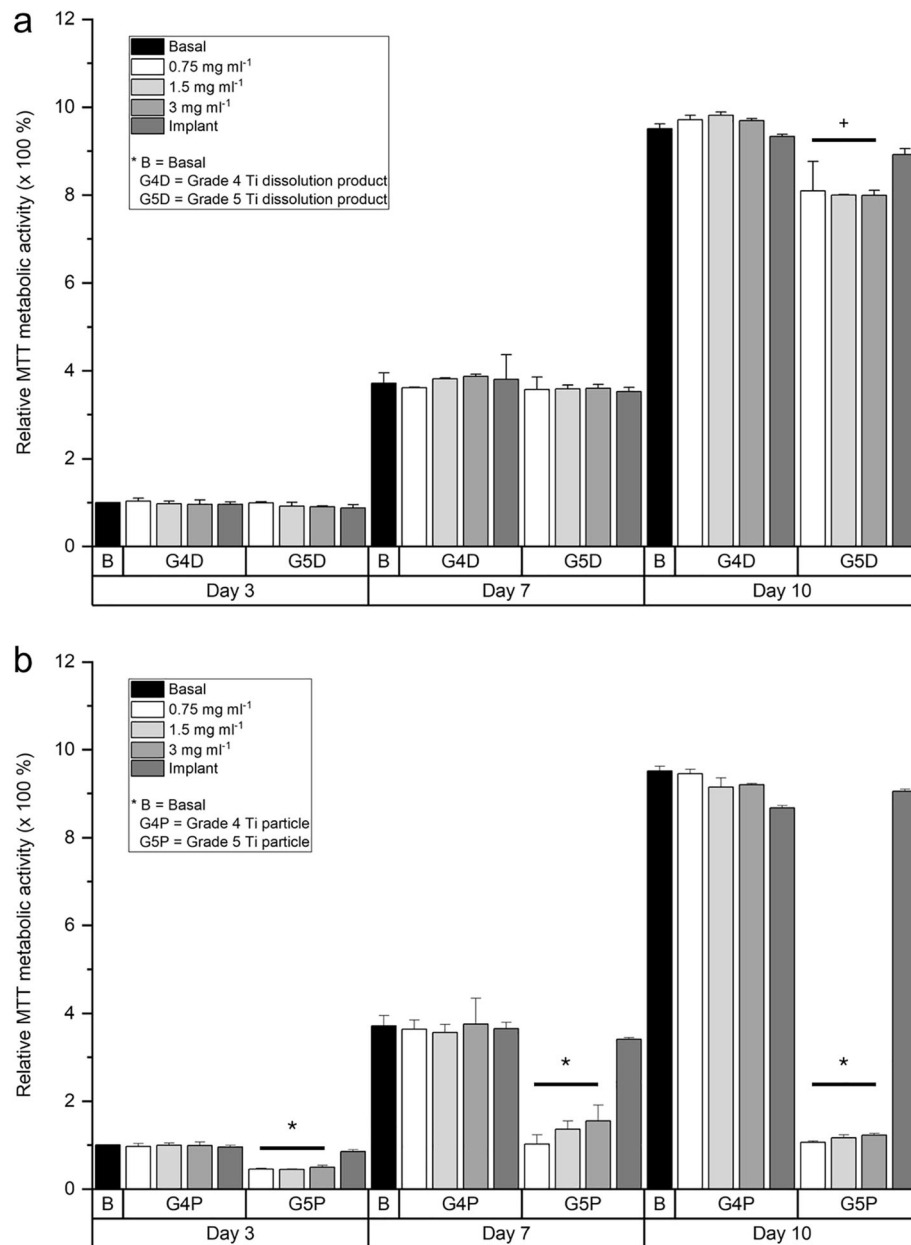
degree of resistance to corrosion of titanium implants [30, 31]. G5 implant particles contain vanadium (Fig. 2), and vanadium ions were released into simulated body fluid and DMEM following 10 days immersion (Fig. 3 and 4).

HGFs exposed to dissolution products of G4 and G5 implant particles did not experience reduction in viability (Fig. 5). This is due to no detectable vanadium release in DMEM by G5 particles during the preparation of the dissolution media, which was 3 days soaking in DMEM (Fig. 4a, b). There was no distinct difference in the amount of titanium ions released from G4 and G5 particles. Direct exposure to G5 implant particles in culture did result in significantly reduced cell viability at all-time points, from 3 to 10 days of culture, while G4 implant particles demonstrated no adverse effect on cell viability (Fig. 5b). The cytotoxic effects of vanadium are well documented [32, 33], so the further relative reduction in cell viability, compared to control and G4 particles, from 10 days was thought to be due to continued release of V during the culture (there was no distinct difference in the amount of titanium ions released from G4 and G5 particles). The delayed release of the V agrees with corrosion studies on Ti-6Al-4 V alloys, which reported time-dependent corrosion [31, 34].

There have been suggestions that sufficient irrigation around the implant and suction of metallic debris during surgical procedures, such as implantoplasty, might reduce the deposition of metallic particles and ions into

surrounding tissue [35]. However, there is no scientific evidence that such measures can fully remove implantoplasty debris from the surround environment, and these procedures can also disseminate bacteria into the surrounding tissues [5, 36]. Previous studies indicated that the cytotoxicity of vanadium ion is dose dependent, where concentrations of 23–30  $\mu$ M (1.17–1.53  $\mu$ g ml<sup>-1</sup>) significantly reduced cell viability in NIH3T3 fibroblasts [33, 37]. Herein, the V concentration was approximately 0.1  $\mu$ g ml<sup>-1</sup> after 10 days of exposure to DMEM, which does explain the significant reduction in viability of HGFs.

Previous studies suggested the viability of calvarial rat osteoblasts in direct contact with G4 CpTi particles (unspecified grade, particle diameter  $3.1 \pm 3.6 \mu$ m) with a concentration higher than 1.5 mg ml<sup>-1</sup> decreased significantly due to rapid phagocytic process [38]. In the present study, the viability of HGFs appeared to be not affected by G4 CpTi implant particles, even at high concentrations (3 mg ml<sup>-1</sup>). This is due to the lack of vanadium and possibly larger particle size. Here, G5 particles are. Although a range of particle size of G5 was measured in this study, a portion of the particles generated from the mock implantoplasty process in the current study is comparable to that reported by Pioletti et al. [38]. The internalisation of G5 particles, especially sub-micron particles, and the subsequent local release of Vanadium ions inside the cytoplasm could increase the toxicity of the particles. A change in pH of culture



**Fig. 5** The effect of grade 4 and grade 5 implant particles on human gingival fibroblast viability in vitro. Viability was determined using an MTT metabolic activity assay. Cells were exposed to either **a** dissolution products (ions and nanoparticles) or **b** culture medium containing suspended implant particles throughout the duration of the culture period. Cells were exposed to various concentrations of particles (0.75, 1.5 or 3 mg ml<sup>-1</sup>). Basal medium and basal medium containing unprocessed dental implants were used as controls. All results were normalized against the value of basal medium at day 3. Results presented as mean  $\pm$  standard deviation,  $n = 3$ . The asterisk indicates  $p < 0.05$ , and  $+$  indicates  $0.05 < p < 0.1$  when compared to basal medium control at each time point

medium was not responsible for the reduced viability as the value of pH was found affect by neither G4 nor G5 implant particles.

As discovered by Malvern Mastersizer and DLS, the sizes of G4 and G5 implant particles released as result of implantoplasty are in the range of nano (NPs) and fine particles (FPs) ( $125.4 \pm 10.9$  nm– $77.4 \pm$

$9.1$   $\mu$ m and  $57.74 \pm 2.66$  nm– $48.4 \pm 6.4$   $\mu$ m for G4 and G5 implant particles, respectively). NPs and FPs can enter cells via a number of routes such as phagocytosis, endocytosis and macropinocytosis as well as passive diffusion [39]. Exposure to nanomaterials and nanoparticles can potentially result in biological responses at molecular level such as DNA methylation,



histone post-translational modifications and noncoding RNAs in mammalian cells [40, 41].

In the field of Orthopaedics, titanium (oxide) wear particles from implants were reported to enter bone-forming cells and stem cells via endocytosis and cause adverse biological response including osteolysis [42–45]. It has also been proposed that titanium particles induce secretion of pro-inflammatory cytokines by fibroblasts, which are involved in the chemotactic migration and recruitment of monocytes/macrophage and subsequently the pathogenesis of aseptic loosening of implants [46]. Therefore, although no short-term effect of G4 particles on HGFs was observed in the present study, further, long-term investigations are also of crucial importance. Further, the effect of implant particles on other cell types within the oral and systemic environments should not be overlooked. Although the health hazards of FPs and NPs are relatively less well established, literature in the fields of toxicology does indicate a glimpse of possible toxicity that should compel clinicians to carefully weigh the possible adverse human health effects. Lastly, “impurities” have been reported in titanium based implant materials, for example, up to 0.5 wt% iron (Fe) in commercial pure titanium (grade 1, 2 and 4) and 0.013 wt% nickel (Ni) (grade 1 and 2) [36, 47, 48]. While these trace metals may not present health risk in a whole implant, ions and particles released as a result of corrosion and/or mechanical intervention such as implantoplasty have been reported to cause adverse allergic reactions in humans [49, 50]. There is no current consensus agreement on the risk of particles released from Ti; however, it would be prudent for clinicians to carefully evaluate the materials used and to consider the potential risks of the individual constituents of any alloy, as indicated in this study.

## Conclusion

In the present study, the release of nano and fine particles from both commercially pure grade 4 titanium and grade 5 Ti-6Al-4 V alloy implants following implantoplasty procedure was reported. Exposure to grade 5 implant particles resulted in significantly reduced cell viability compared to exposure to grade 4 particles. One of the major challenges facing implant dentistry is the lack of information on the possible adverse health effects caused by the exposure to these nano-sized particles. Authors acknowledge that it is inaccurate to directly extrapolate the current findings into human subjects in clinical settings. However, it is probable that the potential toxicity of Ti-6Al-4 V and/or fine implant particles in vivo are also due, at least in part, to the same mechanism presented in the current study. For patient safety, the potential cytotoxicity of Ti-6Al-4 V alloy particles must be considered when used as a material for dental

implants. Furthermore, regardless of implant material, the implantoplasty procedure can release nano-sized particles, the full systemic effect of which is not fully understood. Particles have been shown to have local toxic effects; therefore, the authors do not recommend implantoplasty as a safe procedure for the treatment of peri-implantitis.

## Abbreviations

HGF: Human gingival fibroblasts; G5: Grade 5; SEM: Scanning electron microscopy; SBF: Simulated body fluid; V: Vanadium; C: Carbon; DMEM: Dulbecco's modified Eagle's medium; MTT: 3-(4,5-dimethylthiazol-2-yl)-2,5-Diphenyltetrazolium bromide; DMSO: Dimethyl sulfoxide; ICO-OES: Inductively coupled plasma optical emission spectrometer; CpTi: Commercial pure titanium; G4: Grade 4; DLS: Dynamic light scattering; EDX: Energy dispersive x-ray; Al: Aluminium; Ti: Titanium; FBS: Foetal bovine serum; S.D.: Standard deviation; TiO<sub>2</sub>: Titanium oxide

## Acknowledgements

Authors would like to thank Chelsea Waterhouse (School of Dentistry, University of Central Lancashire) for performing implantoplasty and collecting implant particles.

## Authors' contributions

FB\* contributed to conception, design, data acquisition and interpretation, performed statistical analyses, drafted and critically revised manuscript. SL\* contributed to conception, design, data acquisition, interpretation, performed statistical analyses, drafted and critically revised manuscript. AM contributed to data acquisition. JRJ contributed to conception, design and critically revised manuscript. \*FB and SL contributed equally. All authors gave their final approval and agree to be accountable for all aspects of the work.

## Funding

F. Barrak and S. Li were funded by VSS Ltd (UK).

## Availability of data and materials

The datasets used and/or analysed during the current study are available from [rdm-enquiries@imperial.ac.uk](mailto:rdm-enquiries@imperial.ac.uk) on reasonable request.

## Ethics approval and consent to participate

Not applicable.

## Consent for publication

Not applicable.

## Competing interests

F. Barrak de, S. Li, A. M. Muntane and J. R. Jones declare that they have no competing interests.

## Author details

<sup>1</sup>Department of Materials, Imperial College London, South Kensington Campus, London SW7 2AZ, UK. <sup>2</sup>School of Dentistry, University of Central Lancashire, Preston PR1 2HE, UK.

Received: 11 March 2020 Accepted: 29 July 2020

Published online: 12 September 2020

## References

1. Alrabiah M, Alrahlah A, Al-Hamdan RS, Al-Aali KA, Labban N, Abduljabbar T. Survival of adjacent-dental-implants in prediabetic and systemically healthy subjects at 5-years follow-up. *Clin Implant Dent Relat Res*. 2019; 21(2):232–37.
2. Francetti L, Cavalli N, Taschieri S, Corbella S. Ten years follow-up retrospective study on implant survival rates and prevalence of peri-implantitis in implant-supported full-arch rehabilitations. *Clin Oral Implants Res*. 2019;30(3):252–60.
3. Longhofer LK, Chong A, Strong NM, Wooley PH, Yang SY. Specific material effects of wear-particle-induced inflammation and osteolysis at the bone-implant interface: A rat model. *J Orthop Translat*. 2017;8:5–11.
4. Rivera MC, Perni S, Sloan A, Prokopovich P. Anti-inflammatory drug-eluting implant model system to prevent wear particle-induced periprosthetic osteolysis. *Int J Nanomedicine*. 2019;14:1069–84.

5. Delgado-Ruiz R, Romanos G. Potential causes of titanium particle and ion release in implant dentistry: a systematic review. *Int J Mol Sci*. 2018;19(11):3585–621.
6. Senna P, Antoninha Del Bel Cury A, Kates S, Meirelles L. Surface damage on dental implants with release of loose particles after insertion into bone. *Clin Implant Dent Relat Res*. 2015;17(4):681–92.
7. Siirila HS, Kononen M. The effect of oral topical fluorides on the surface of commercially pure titanium. *Int J Oral Maxillofac Implants*. 1991;6(1):50–4.
8. Mabilieu G, Bourdon S, Joly-Guillou ML, Filmon R, Basle MF, Chappard D. Influence of fluoride, hydrogen peroxide and lactic acid on the corrosion resistance of commercially pure titanium. *Acta Biomater*. 2006;2(1):121–9.
9. Barbieri M, Mencio F, Papi P, Rosella D, Di Carlo S, Valente T, et al. Corrosion behavior of dental implants immersed into human saliva: preliminary results of an in vitro study. *Eur Rev Med Pharmacol Sci*. 2017;21(16):3543–8.
10. Prathapachandran J, Suresh N. Management of peri-implantitis. *Dent Res J (Isfahan)*. 2012;9(5):516–21.
11. Berglundh T, Armitage G, Araujo MG, Avila-Ortiz G, Blanco J, Camargo PM, et al. Peri-implant diseases and conditions: consensus report of workgroup 4 of the 2017 World Workshop on the Classification of Periodontal and Peri-Implant Diseases and Conditions. *J Periodontol*. 2018;89(Suppl 1):S313–S8.
12. Berglundh T, Persson L, Klinge B. A systematic review of the incidence of biological and technical complications in implant dentistry reported in prospective longitudinal studies of at least 5 years. *J Clin Periodontol*. 2002;29(Suppl 3):197–212 discussion 32–3.
13. Derks J, Tomasi C. Peri-implant health and disease. A systematic review of current epidemiology. *J Clin Periodontol*. 2015;42(Suppl 16):S158–71.
14. Derks J, Schaller D, Hakansson J, Wennstrom JL, Tomasi C, Berglundh T. Effectiveness of implant therapy analyzed in a Swedish population: prevalence of peri-implantitis. *J Dent Res*. 2016;95(1):43–9.
15. Mombelli A, Muller N, Cionca N. The epidemiology of peri-implantitis. *Clin Oral Implants res*. 2012;23(Suppl 6):67–76.
16. Lang NP, Wilson TG, Corbet EF. Biological complications with dental implants: their prevention, diagnosis and treatment. *Clin Oral Implants Res*. 2000;11(Suppl 1):146–55.
17. Flanagan D. Bite force and dental implant treatment: a short review. *Med Devices (Auckl)*. 2017;10:141–8.
18. Ferreira SD, Silva GL, Cortelli JR, Costa JE, Costa FO. Prevalence and risk variables for peri-implant disease in Brazilian subjects. *J Clin Periodontol*. 2006;33(12):929–35.
19. Lindhe J, Meyle J. Group DoEwOP. Peri-implant diseases: Consensus Report of the Sixth European Workshop on Periodontology. *J Clin Periodontol*. 2008;35(8 Suppl):282–5.
20. Albrektsson T, Canullo L, Cochran D, De Bruyn H. "Peri-Implantitis": a complication of a foreign body or a man-made "Disease". Facts and Fiction. *Clin Implant Dent Relat Res*. 2016;18(4):840–9.
21. Tawse-Smith A, Ma S, Wu H, Yeah A. Changes in surface characteristics of moderately roughened grade IV titanium disk following a standardised implantoplasty technique: an in-vitro study. *Braz J Periodontol*. 2015;25:22–33.
22. Gehrke SA, Aramburu Junior JS, Dedavid BA, Shibli JA. Analysis of implant strength after implantoplasty in three implant-abutment connection designs: an in vitro study. *Int J Oral Maxillofac Implants*. 2016;31(3):e65–70.
23. Macon AL, Kim TB, Valliant EM, Goetschius K, Brow RK, Day DE, et al. A unified in vitro evaluation for apatite-forming ability of bioactive glasses and their variants. *J Mater Sci Mater Med*. 2015;26(2):115.
24. Kokubo T, Kushitani H, Sakka S, Kitsugi T, Yamamuro T. Solutions able to reproduce in vivo surface-structure changes in bioactive glass-ceramic A-W. *J Biomed Mater Res*. 1990;24(6):721–34.
25. Macon ALB, Kim TB, Valliant EM, Goetschius K, Brow RK, Day DE, et al. A unified in vitro evaluation for apatite-forming ability of bioactive glasses and their variants. *Journal of Materials Science: Materials in Medicine*. 2015;26(2):115.
26. McCracken M. Dental implant materials: commercially pure titanium and titanium alloys. *J Prosthodont*. 1999;8(1):40–3.
27. UK SMCL. Ti-6Al-4V (Grade 5) Technical Datasheet. 2018.
28. UK SMCL. CP Grade 4 Technical Datasheet. 2018.
29. Palmquist A, Omar OM, Esposito M, Lausmaa J, Thomsen P. Titanium oral implants: surface characteristics, interface biology and clinical outcome. *J R Soc Interface*. 2010;7(Suppl 5):S515–27.
30. Addison O, Davenport AJ, Newport RJ, Kalra S, Monir M, Mosselmans JF, et al. Do 'passive' medical titanium surfaces deteriorate in service in the absence of wear? *J R Soc Interface*. 2012;9(76):3161–4.
31. Zhang Y, Addison O, Yu F, Troconis BCR, Scully JR, Davenport AJ. Time-dependent enhanced corrosion of Ti6Al4V in the presence of H<sub>2</sub>O<sub>2</sub> and albumin. *Sci Rep*. 2018;8(1):3185.
32. Sargeant A, Goswami T, Swank M. Ion concentrations from hip implants. *J Surg Orthop Adv*. 2006;15(2):113–4.
33. Costa BC, Tokuhara CK, Rocha LA, Oliveira RC, Lisboa-Filho PN, Costa PJ. Vanadium ionic species from degradation of Ti-6Al-4V metallic implants: in vitro cytotoxicity and speciation evaluation. *Mater Sci Eng C Mater Biol Appl*. 2019;96:730–9.
34. Rodrigues DC, Urban RM, Jacobs JJ, Gilbert JL. In vivo severe corrosion and hydrogen embrittlement of retrieved modular body titanium alloy hip-implants. *J Biomed Mater Res B Appl Biomater*. 2009;88(1):206–19.
35. Rashad A, Sadr-Eshkevari P, Weuster M, Schmitz I, Prochnow N, Maurer P. Material attrition and bone micromorphology after conventional and ultrasonic implant site preparation. *Clin Oral Implants Res*. 2013;24(Suppl A100):110–4.
36. Rosen PS, Qari M, Froum SJ, Dibart S, Chou LL. A pilot study on the efficacy of a treatment algorithm to detoxify dental implant surfaces affected by peri-implantitis. *Int J Periodontics Restorative Dent*. 2018;38(2):261–7.
37. Hallab NJ, Mikecz K, Vermes C, Skipor A, Jacobs JJ. Orthopaedic implant related metal toxicity in terms of human lymphocyte reactivity to metal-protein complexes produced from cobalt-base and titanium-base implant alloy degradation. *Mol Cell Biochem*. 2001;222(1-2):127–36.
38. Pioletti DP, Takei H, Kwon SY, Wood D, Sung KL. The cytotoxic effect of titanium particles phagocytosed by osteoblasts. *J Biomed Mater Res*. 1999;46(3):399–407.
39. Behzadi S, Serpooshan V, Tao W, Hamaly MA, Alkawareek MY, Dreaden EC, et al. Cellular uptake of nanoparticles: journey inside the cell. *Chem Soc Rev*. 2017;46(14):4218–44.
40. Sierra MI, Valdes A, Fernandez AF, Torrecillas R, Fraga MF. The effect of exposure to nanoparticles and nanomaterials on the mammalian epigenome. *Int J Nanomedicine*. 2016;11:6297–306.
41. Albulescu R, Popa AC, Enciu AM, Albulescu L, Dudau M, Popescu ID, et al. Comprehensive in vitro testing of calcium phosphate-based bioceramics with orthopedic and dentistry applications. *Materials (Basel)*. 2019;12(22):3704–45.
42. Haleem-Smith H, Argintar E, Bush C, Hampton D, Postma WF, Chen FH, et al. Biological responses of human mesenchymal stem cells to titanium wear debris particles. *J Orthop Res*. 2012;30(6):853–63.
43. Okafor CC, Haleem-Smith H, Laqueriere P, Manner PA, Tuan RS. Particulate endocytosis mediates biological responses of human mesenchymal stem cells to titanium wear debris. *J Orthop Res*. 2006;24(3):461–73.
44. Yao JJ, Lewallen EA, Trousdale WH, Xu W, Thaler R, Salib CG, et al. Local cellular responses to titanium dioxide from orthopedic implants. *Biores Open Access*. 2017;6(1):94–103.
45. Gargioli C, Turturici G, Barreca MM, Spinello W, Fuoco C, Testa S, et al. Oxidative stress preconditioning of mouse perivascular myogenic progenitors selects a subpopulation of cells with a distinct survival advantage in vitro and in vivo. *Cell Death Dis*. 2018;9(1):1.
46. Wu W, Wang L, Mao YQ, Dai KR, Hao YQ. Impaired Autophagy in the fibroblasts by titanium particles increased the release of CX3CL1 and promoted the chemotactic migration of monocytes. *Inflammation*. 2020;43(2):673–85.
47. ASM Aerospace Specification Metals Inc - Titanium Grade 4 specification sheet (Web access) [Available from: <http://asm.matweb.com/search/SpecificMaterial.asp?bassnum=MTU040>].
48. Boyer R, Welsch G, Collings W. *Materials Properties Handbook: Titanium Alloys*. ASM International: Ohio; 1994.
49. Harloff T, Hönle W, Holzwarth U, Bader R, Yhomas P, Schuh A. Titanium allergy or not? "Impurity" of titanium implant materials. *Health*. 2010;2(4):306–10.
50. Chaturvedi T. Allergy related to dental implant and its clinical significance. *Clin Cosmet Investig Dent*. 2013;5:57–61.

## Publisher's Note

Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.